

# Biomechanics of Meniscal Allograft Transplantation: A Meta-Analysis

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## SUMMARY

**Introduction.** Despite trends to repair meniscal defects, meniscectomy continues to be a common procedure. Degenerative changes following these surgeries become candidates for meniscal allograft transplantation.

**Purpose.** The purpose of this meta-analysis was to review published articles that compared methods of meniscal allograft transplantation (bone plug, suture only, or bone bridge) for their biomechanical effects on tibiofemoral mean contact pressure and contact area in relation to intact meniscal states.

**Materials and methods.** PubMed database search on July 15, 2020 for articles evaluating the knee kinematics of MAT in a biomechanical model.

**Results.** The greatest contact area was found in the setting of an intact meniscal state, with a mean difference of 188.886 mm<sup>3</sup> (95%CI 148.059-229.672,  $p < 0.001$ ) and 78.713 (95%CI 78.713-103.733,  $p < 0.001$ ), when compared to meniscectomy and MAT respectively. Although MAT showed a lower contact area *vs* the intact knee, it did have a greater contact area than meniscectomy by 94.951 mm<sup>2</sup> (95%CI, 71.590-118.312,  $p < 0.001$ ). The dovetail bone bridge technique was shown to have the highest difference in mean contact area of 207.676 mm<sup>2</sup> (95%CI 85.288-330.065,  $p < 0.001$ ) when compared to bone plug technique.

**Conclusions.** Meniscal allograft transfer demonstrated significantly less contact area than a meniscus intact knee and significantly higher contact area than meniscectomy. In the systematic review, bone bridge meniscal allograft transplant techniques offered the closest reproduction of native knee biomechanics when compared to bone plug and suture only.

## KEY WORDS

*Meniscal allograft transplant techniques; biomechanics; contact area; meniscus; meniscectomy.*

## INTRODUCTION

The meniscus is a fibrocartilaginous tissue that reduces tibiofemoral contact forces by increasing joint congruency. Additionally, it serves as a source of proprioception, nutrition, and lubrication (1-4). Originally described by Fairbanks, complete meniscectomy rapidly increased the rate of osteoarthritis within the knee. Indeed, it is well established in the literature that meniscal deficiency leads to mechanical knee degeneration (5-9). Although there have been more recent trends to preserve the damaged meniscus with repair techniques, meniscectomy contin-

ues to be a commonly employed procedure when repair is not feasible (10-14). Certain tear morphologies consisting of flaps, radial tears, and large degenerative tears are largely considered irreparable (15, 16). Unfortunately, these injuries frequently leave patients with subtotal or total meniscectomy. Young patients with symptomatic degenerative changes following these surgeries become candidates for meniscal allograft transplantation. Since the original case series by Milachowski *et al.*, meniscal allograft transplantation (MAT) has become an acceptable method of treating young patients with chal-

lenging meniscal deficiency. MAT success is dependent on numerous variables: graft size, knee stability, degree of arthrosis, axial alignment, rehabilitation protocol, and obesity. Recent studies have shown fair to excellent outcomes, second look arthroscopies have demonstrated healing to the peripheral rim, and some series have shown 70% clinical survivorship at 10 years postoperatively (2, 17-22). The most important surgeon controllable factor is the method of MAT fixation. To date there exist three methods of MAT: 1) dovetail bone bridge fixation - in which the posterior and anterior horns of the graft remain connected to a single piece of bone, 2) bone plug fixation - in which 2 separate osseous segments are attached to the posterior and anterior horns, 3) suture only - in which the meniscal allograft is tethered to the meniscocapsular rim via suture fixation. Various studies have demonstrated alteration in joint contact forces with these different fixation techniques; however there remains no literature directly comparing these methods across studies (18-20, 22-27).

The purpose of this meta-analysis was to review published articles that compared methods of meniscal allograft transplantation (bone plug, suture only, or bone bridge) for their biomechanical effects on tibiofemoral mean contact pressure and contact area in relation to intact meniscal states.

## MATERIALS AND METHODS

There were no ethical concerns for this meta-analysis of biomechanical articles.

### Article screening

We searched the PubMed database on July 15, 2020 for articles evaluating the knee kinematics of MAT in a biomechanical model. The search field was entered as: (“Meniscus allograft”[All Fields] OR “Meniscal allograft”[All Fields] OR “meniscus allograft transplant”[all fields] or “meniscal allograft transplant”[all fields]) AND (“Biomechanic”[All Fields] OR “Biomechanics”[All Fields] OR “Biomechanical”[All Fields] OR “cadaver”[all fields]). Two authors (BC and KP) independently screened the resulting 85 articles for inclusion or exclusion using Abstrackr software (Brown, Providence, RI). Disagreements were reviewed by the lead author (SK) who made the final decision whether to include or exclude the references. Inclusion criteria were biomechanical studies of MAT on human cadavers that reported mean contact area, mean contact pressure, mean peak contact pressure in native, total meniscectomy states as well as following MAT. Initial screening following a review of disagree-

ments resulted in 15 articles for full review. The sources of these articles were reviewed and cross-referenced with the 85 original articles. Five additional articles were added to the full text review while seven were excluded for different reasons such as only reporting translation/strain forces, pull out strength, extrusion values and lack of mean and standard deviation values. Subsequently 12 articles were included in the study. These articles were then evaluated for quality using the Quality Appraisal for Cadaveric Studies (QUACS) scale, which is a validated means for assessing the quality of cadaveric studies.

### Data collection and included studies

Data was collected from each including: sample size, mean contact pressure, mean peak contact pressure, mean contact area, MAT fixation type, force applied during testing, MAT location (medial *vs* lateral) and graft type. The included studies were Ambra, Brial, Dienst, Huang, Huang, Kim, McDermott, Paletta, Sekaren, Vrancken, Wang.

## RESULTS

The results of the meta-analysis showed that the greatest contact area was found in the setting of an intact meniscal state, with a mean difference of 188.886 mm<sup>3</sup> (95%CI 148.059-229.672,  $p < 0.001$ ) and 78.713 (95%CI 78.713-103.733,  $p < 0.001$ ), when compared to meniscectomy and MAT respectively. Although MAT showed a lower contact area *vs* the intact knee, it did have a greater contact area than meniscectomy by 94.951 mm<sup>2</sup> (95%CI, 71.590-118.312,  $p < 0.001$ ) (**table I**).

Regarding mean contact pressure and mean peak contact pressure, meniscectomy had greater pressures *vs* MAT by 0.506 MPa (95%CI 0.351-0.660,  $p < 0.001$ ) and intact states by 0.751 (95%CI 0.549-0.952,  $p < 0.001$ ). MAT also was noted to have a greater mean contact and mean peak contact pressures than intact states by 0.239 Mpa (95%CI 0.145-0.332,  $p < 0.001$ ) (**table II**).

Meta-regression showed that each of the MAT techniques chosen had differing effect on contact area and contact pressures (**table III**). The dovetail bone bridge technique was shown to have the highest difference in mean contact area of 207.676 mm<sup>2</sup> (95%CI 85.288-330.065,  $p < 0.001$ ) when compared to bone plug technique. There was also a greater difference of 115.250 mm<sup>2</sup> (95 CI 40.761-189.740,  $p = 0.002$ ) in the contact area of soft tissue grafts in comparison to bone plug technique. Additionally, the soft tissue graft had the lowest difference in mean contact pressure of 1.018 MPa (95%CI -1.688 to -0.347,

p = 0.003) less than the bone plug technique. Inconsequentially, bone plug was shown to have the lowest peak contact pressure of 5.525 MPa (95%CI 4.923-6.126) with

differences between dovetail and soft tissue graft being 2.074 (-0.027 to 4.175, p = 0.053) and 0.848 (-0.347 to 2.043, p = 0.164).

**Table I.** Characteristics of included studies.

| Lead Author | Year of Publication | Technique                             | Compartment | Total Sample Size | Average Age Cadavers (Years) |
|-------------|---------------------|---------------------------------------|-------------|-------------------|------------------------------|
| Ambra       | 2019                | Bone plug <i>vs</i> suture only       | Medial      | 9                 | 46.9                         |
| Brial       | 2019                | Bone bridge <i>vs</i> bone plug       | Lateral     | 6                 | Not Reported                 |
| Dienst      | 2007                | Bone bridge                           | Lateral     | 6                 | 66 (49-79)                   |
| Huang       | 2002                | Bone plug                             | Lateral     | 15                | 52                           |
| Kim         | 2012                | Suture only                           | Medial      | 10                | 54 (42-61)                   |
| McDermott   | 2008                | Bone bridge <i>vs</i> suture only     | Lateral     | 5                 | 89                           |
| Paletta     | 1997                | Bone plug                             | Lateral     | 10                | 22-47 (avg not reported)     |
| Sekaren     | 2002                | Bone Plug                             | Medial      | 8                 | 56 (38-70)                   |
| Vrancken    | 2014                | Suture only (PCU <i>vs</i> allograft) | Medial      | 5                 | 70-88                        |
| Wang        | 2014                | Bone plug <i>vs</i> suture only       | Medial      | 7                 | Not Reported                 |
| Alhalki     | 2000                | Bone Plug (Allo <i>vs</i> Auto)       | Medial      | 10                | 70                           |
| Alhalki     | 1999                | Bone plug <i>vs</i> suture            | Medial      | 10                | 70                           |

**Table II.** Statistical analysis.

| Comparison   | Difference in Mean Contact Area (mm <sup>2</sup> ) (95%CI) | P value |
|--|--|---------|
| Intact <i>vs</i> Meniscectomy                          | 188.866 (148.059-229.672)                                  | < 0.001 |
| MAT <i>vs</i> Meniscectomy                             | 94.951 (71.590-118.312)                                    | < 0.001 |
| Intact <i>vs</i> MAT                                   | 78.713 (53.694-103.733)                                    | < 0.001 |
| Difference in Mean Contact Pressure (MPa) (95%CI)      |  |         |
| Meniscectomy <i>vs</i> Intact                          | 0.751 (0.549-0.952)  | < 0.001 |
| Meniscectomy <i>vs</i> MAT                             | 0.506 (0.351-0.660)  | < 0.001 |
| MAT <i>vs</i> Intact                                   | 0.239 (0.145-0.332)  | < 0.001 |
| Difference in Mean Peak Contact Pressure (MPa) (95%CI) |  |         |
| Meniscectomy <i>vs</i> Intact                          | 2.730 (1.850-3.610)  | < 0.001 |
| Meniscectomy <i>vs</i> MAT                             | 1.129 (0.538-1.720)  | < 0.001 |
| MAT <i>vs</i> Intact                                   | 1.676 (0.869-2.482)  | < 0.001 |

**Table III.** Meta regression.

| Contact Area (mm <sup>2</sup> )                  |
|--|
| Bone plug 248.336 (209.345-287.328)              |
| Dovetail +207.676 (85.288-330.065) p < 0.001     |
| Soft tissue +115.250 (40.761-189.740) p = 0.002  |
| Medial 377.123 (328.865-425.381)                 |
| Lateral -146.367 (-210.082 to -82.651) p < 0.001 |
| All MATs medial and lateral                      |
| Mean Contact Pressure                            |
| Bone plug 2.213 (1.876-2.550)                    |
| Dovetail -0.923 (-2.662-0.816) p = 0.298         |
| Soft tissue -1.018 (-1.688 to -0.347) p = 0.003  |
| Medial 1.297 (0.938-1.656)                       |
| Lateral +1.239 (0.733-1.746) p < 0.001           |
| Peak Contact Pressure                            |
| Bone Plug 5.525 (4.923-6.126)                    |
| Dovetail +2.074 (-0.027-4.175) p = 0.053         |
| Soft tissue +0.848 (-0.347- 2.043) p = 0.164     |
| Medial 5.125 (4.301- 5.949)                      |
| Lateral +1.177 (0.132-2.222) p = 0.027           |

## DISCUSSION

### Main findings of our paper

#### *Intact vs MAT vs meniscectomy and purpose of meta-analysis*

In agreement with prior literature on the topic, the meniscal allograft transplant does not restore knee biomechanics to a native state (2, 18, 20, 22, 24, 28). When compared to complete meniscectomy, meniscal allograft transplant in our review demonstrated improvement in contact area by 94.9 mm<sup>2</sup>, which corresponded to a decrease in both mean contact pressures and mean peak pressures by 0.506 and 1.129 MPa – respectively. These findings reinforce that MAT improves knee biomechanics by increasing contact area. Although the contact area and pressures after MAT more closely approach those of an intact knee state, there remains a statistically significant difference when compared to an intact knee. These findings support the significant role of the meniscus as a load distributor within the knee and explains the correlation between degenerative changes and meniscal deficiency (13, 29-32). Additionally, Zaffagini *et al.* found that knee laxity was reduced following MAT compared to the pre-operative state, indicating a role for MAT in improving the biomechanics of the knee (33). As the body of evidence on meniscal allograft transplantation

continues to grow, the gap between biomechanics of the meniscal transplanted knee and native knee may continue to shrink (1, 22, 24, 25).

The 12 high-quality biomechanical studies included in our systematic review determined that meniscal allograft transplantation through a dovetail bone bridge graft technique was shown to have a statistically significant higher contact area than bone plug and suture only techniques. Furthermore, the mean peak contact pressures encountered through bone plug techniques were lower than both dovetail and soft tissue techniques, although the difference between bone plug and soft tissue was not statistically significant. These are important variables to take into consideration when discussing surgical indications and techniques for meniscal allograft transplantation (2, 24). A pitfall of any MAT procedure is the size of the chondral defect, which is difficult to remedy no matter the technique. Steadman microfracture technique aims to fill the chondral defect with stable clot, thereby providing an ideal environment for repair. This technique has been shown to be effective in the management of high-grade chondral defects with great clinical outcomes at 11-year follow-up (34). No biomechanical studies have been performed to assess whether Steadman microfracture technique is able to restore knee biomechanics to a native state. The authors feel future research should target this question.

### Contact area

Upon meta regression, meniscal allograft transplantation through dovetail bone bridge technique had the greatest increase in compartment contact area compared to traditional bone plug by 207.676 mm<sup>2</sup> (95%CI 85.288-330.065)  $p < 0.001$  and soft tissue grafts by 115.250 mm<sup>2</sup> (95%CI 40.761-189.740)  $p = 0.002$ . Although these values still significantly fell short of the native knee by an average of 78 mm<sup>2</sup>.

In comparison to previous literature, our results corroborate the role of boney techniques in achieving rigid fixation of both the anterior and posterior horns – particularly the dovetail MAT, which was closest to restoring contact area in comparison to an intact knee. For example, Ambra *et al.* was not able to demonstrate significant difference in mean contact area between MAT with bone plug and native knee states, but suture only fixation was significantly associated with reduced contact area compared to native knee state within 0-30 degrees of flexion (28). Similarly, Wang *et al.* showed MAT via bone plugs resulted in increased contact area that more closely resembled native knee state than with MAT via suture only fixation (38). These differences in contact area from varying MAT techniques are likely the result of the degree of meniscal extrusion throughout dynamic knee activities. In fact, rigid fixation is an essential tenet to avoid meniscal extrusion under increasing axial loads (35). While technically easier, it remains controversial if soft-tissue-only fixation is comparable to boney techniques, as few biomechanical studies exist directly comparing the two (28). For example, one series citation found suture only to have a lower contact area than bone plug, but the difference was not statistically significant (36). Additionally, Alhalki *et al.* demonstrated no significant difference in medial knee contact area compared to native knee after MAT with bone plug or with suture (36).

### Mean contact pressure/peak contact pressure

Our values for peak contact pressure correlate with established literature. Alhalki *et al.* showed that neither MAT with bone plug nor MAT with suture reconstituted normal medial knee peak contact pressures; however, normalized peak pressures were significantly higher when using a suture only technique. Furthermore, mean pressures were not significantly different from MAT with bone plug *versus* normal knee states, but were significantly greater with suture only technique (49-61% increased pressure throughout knee ROM 0-45 degrees) (36). McDermott *et al.* was not able to demonstrate a significant difference in peak contact pressures between MAT via bone block or MAT via suture compared to native knee states; however, direct comparison of peak pressures showed significant increase in suture only

compared to bone block techniques (32). Similarly, Wang *et al.* and Ambra *et al.* demonstrated closer approximation of native knee contact and peak contact pressures with bone plug techniques as compared to soft tissue techniques.

Interestingly, meta regression revealed mean contact pressures were lowest with soft tissue techniques by 1.018 Mpa ( $p = 0.003$ ) compared to bone plug and no significant difference between either of the boney techniques. These findings, however, are likely contributed to the great heterogeneity within studies. Of the 12 included studies for meta-analysis, only 4 directly compared boney to soft tissue procedures (28, 32, 36, 38), while 2 reported values exclusively for suture techniques (30, 39). Sub stratification of compartmental peak contact pressures by MAT technique demonstrated lowest pressures with bone plug (5.525 MPa) technique, which was not statistically different from dovetail (7.599,  $p = 0.053$ ) or soft tissue techniques (Mpa = 6.373,  $p = 0.164$ ).

### Biomechanical comparisons between MAT techniques with consideration of medial vs lateral compartments

Direct comparison of medial *versus* lateral compartments after MAT did demonstrate that medial compartment more frequently had greater contact area, lower contact pressure, and lowest peak contact pressures. These results are consistent both with prior literature and native knee biomechanics. For example, Devaraj *et al.* discussed that the ability of the medial condyle to withstand greater forces is due to the more constrained medial meniscus as it is attached to the MCL (37). This necessitates a greater contact area as the medial condyle functions as the central point of pressure during the knee is in extension. Dynamically, when flexion is involved, the medial meniscus posteriorly carries loads during the early stance phase of walking. Because the asymmetric C-shape, the anterior portion of the medial meniscus is much thinner anteriorly and less readily absorbs the joint load compared with the posterior area (38). This inherently makes direct comparison of soft tissue techniques in the lateral meniscus more challenging.

The previous literature in consideration of the lateral compartment, has predominately focused on the biomechanical advantages that can be gained. It has been postulated that in order to gain biomechanical advantage with a MAT procedure, the circumferential distribution of axial loads by the menisci must be taken into account. This particularly applies to the allograft attachment to the anterior and posterior meniscal horns (40). Due to the proximity of the anterior and posterior horns of the lateral meniscus, some authors favor bone bridge fixation of the lateral compartment while more variability exists in medial compartment techniques (41).

## Limitations

Anatomic meniscal allograft transplantation is a challenging procedure requiring technical precision. Indeed, it has been demonstrated in cadaveric studies that nonanatomic placement exceeding 5 mm has dramatic effects on contact pressures (42). This bears reason on clinicians frequently using size matched transplants when performing these procedures but was not the case for the studies mentioned. These cadaveric studies were frequently performed in a manner where external validity of accurate horn positioning was not always possible. This also brings into question the difference in protocols for each study and the lack of control groups used within.

The precise relationship between contact stress and area to articular cartilage longevity has not been determined (43). Numerous clinical studies have been published demonstrating a variety of surgical techniques and their clinical outcomes but still have not highlighted a particular advantage of bony to suture technique (26, 27, 44-47). Nonetheless it is generally regarded that biomechanical forces withstood by the tibiofemoral surface plays an important role in joint degradation (48-50). It should also be noted that despite any biomechanical limitations of MAT, graft survivorship at 10 years has been shown to be as high as 89% (51).

## CONCLUSIONS

In conclusion, this meta-analysis showed that meniscal allograft transfer demonstrated a significantly higher contact area than meniscectomy. However, it still had significantly less contact area than a meniscus intact knee.

## REFERENCES

1. Caldwell GL, Allen AA, Fu FH. Functional anatomy and biomechanics of the meniscus. *Oper Tech Sports Med.* 1994;2(3):152-63. doi: 10.1016/1060-1872(94)90013-2.
2. Matava MJ. Meniscal allograft transplantation: a systematic review. *Clin Orthop Relat Res.* 2007;455:142-57. doi: 10.1097/BLO.0b013e318030c24e.
3. Cameron HU, Macnab I. The structure of the meniscus of the human knee joint. *Clin Orthop Relat Res.* 1972;89:215-9. doi: 10.1097/00003086-197211000-00028.
4. Fox AJS, Wanivenhaus F, Burge AJ, Warren RF, Rodeo SA. The human meniscus: a review of anatomy, function, injury, and advances in treatment. *Clin Anat.* 2015;28(2):269-87. doi: 10.1002/ca.22456.
5. Fairbank TJ. Knee joint changes after meniscectomy. *J Bone Joint Surg Br.* 1948;30B(4):664-70. doi: 10.1302/0301-620X.30B4.664.
6. Carbone A, Rodeo S. Review of current understanding of post-traumatic osteoarthritis resulting from sports injuries. *J Orthop Res.* 2017;35(3):397-405. doi: 10.1002/jor.23341.
7. Lohmander LS, Englund PM, Dahl LL, Roos EM. The long-term consequence of anterior cruciate ligament and meniscus injuries: osteoarthritis. *Am J Sports Med.* 2007;35(10):1756-69. doi: 10.1177/0363546507307396.
8. McCann L, Ingham E, Jin Z, Fisher J. Influence of the meniscus on friction and degradation of cartilage in the natural knee joint. *Osteoarthr Cartil.* 2009;17(8):995-1000. doi: 10.1016/j.joca.2009.02.012.
9. Rangger C, Klestil T, Gloetzer W, Kemmler G, Benedetto KP. Osteoarthritis after arthroscopic partial meniscectomy. *Am J Sports Med.* 1995;23(2):240-4. doi: 10.1177/036354659502300219.

Consequentially, to reduce biomechanical burden through improving MAT techniques, we sought to better elucidate which is optimal among the three current methods of MAT: dovetail bone bridge, bone plug, and suture only. In this systematic review, dovetail bone bridge meniscal allograft transplant techniques offered the closest reproduction of native knee biomechanics with the significantly highest mean contact area. Although this cadaveric biomechanical evidence suggests an advantage in reproduction of native knee biomechanics with bony techniques in MAT, the clinical studies thus far do not demonstrate superiority with any technique. Further prospective study is necessary to understand the effects of MAT on native biomechanics.

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None.

## DATA AVAILABILITY

Data are available under reasonable request to the corresponding author.

## CONTRIBUTIONS

SK, KP, BC: data collection, writing - original draft, writing - review & editing. NR: writing - original draft, writing - review & editing. EH: data analysis, writing - original draft, writing - review & editing.

## CONFLICT OF INTERESTS

The authors declare that they have no conflict of interests.

10. Baker BE, Peckham AC, Puppato F, Sanborn JC. Review of meniscal injury and associated sports. *Am J Sports Med.* 1985;13(1):1-4. doi: 10.1177/036354658501300101.
11. Jackson DW. Reconstructive Knee Surgery. *J Orthop Trauma.* 1995;9(3):277. doi: 10.1097/00005131-199506000-00020.
12. Abrams GD, Frank RM, Gupta AK, Harris JD, McCormick FM, Cole BJ. Trends in meniscus repair and meniscectomy in the United States, 2005-2011. *Am J Sports Med.* 2013;41(10):2333-9. doi: 10.1177/0363546513495641.
13. Sommerlath KG. Results of meniscal repair and partial meniscectomy in stable knees. *Int Orthop.* 1991;15(4):347-50. doi: 10.1007/BF00186875.
14. Shelbourne KD, Carr DR. Meniscal repair compared with meniscectomy for bucket-handle medial meniscal tears in anterior cruciate ligament-reconstructed knees. *Am J Sports Med.* 2003;31(5):718-23. doi: 10.1177/03635465030310051401.
15. Laible C, Stein DA, Kiridly DN. Meniscal repair. *J Am Acad Orthop Surg.* 2013;21(4):204-13. doi: 10.5435/JAAOS-21-04-204.
16. Taylor SA, Rodeo SA. Augmentation techniques for isolated meniscal tears. *Curr Rev Musculoskelet Med.* 2013;6(2):95-101. doi: 10.1007/s12178-013-9165-z.
17. Milachowski KA, Weismeier K, Wirth CJ. Homologous meniscus transplantation. Experimental and clinical results. *Int Orthop.* 1989;13(1):1-11. doi: 10.1007/BF00266715.
18. Rijk PC. Meniscal allograft transplantation--part I: background, results, graft selection and preservation, and surgical considerations. *Arthroscopy.* 2004;20(7):728-43. doi: 10.1016/j.arthro.2004.06.015.
19. Verdonk R, Volpi P, Verdonk P, et al. Indications and limits of meniscal allografts. *Injury.* 2013;44 Suppl 1:S21-7. doi: 10.1016/S0020-1383(13)70006-8.
20. Hergan D, Thut D, Sherman O, Day MS. Meniscal allograft transplantation. *Arthroscopy.* 2011;27(1):101-12. doi: 10.1016/j.arthro.2010.05.019.
21. Brophy RH, Matava MJ. Surgical options for meniscal replacement. *J Am Acad Orthop Surg.* 2012;20(5):265-72. doi: 10.5435/JAAOS-20-05-265.
22. Rijk PC. Meniscal allograft transplantation--part II: alternative treatments, effects on articular cartilage, and future directions. *Arthroscopy.* 2004;20(8):851-9. doi: 10.1016/j.arthro.2004.07.010.
23. Lee YHD, Caborn DNM. A new technique for arthroscopic meniscus transplant using soft tissue fixation and anatomical meniscal root reinsertion. *Knee Surg Sports Traumatol Arthrosc.* 2012;20(5):904-8. doi: 10.1007/s00167-011-1647-1.
24. Peters G, Wirth CJ. The current state of meniscal allograft transplantation and replacement. *Knee.* 2003;10(1):19-31. doi: 10.1016/s0968-0160(02)00139-4.
25. Rodeo SA. Meniscal allografts--where do we stand? *Am J Sports Med.* 2001;29(2):246-61. doi: 10.1177/03635465010290022401.
26. Shelton WR, Dukes AD. Meniscus replacement with bone anchors: a surgical technique. *Arthroscopy.* 1994;10(3):324-7. doi: 10.1016/s0749-8063(05)80122-7.
27. Woodmass JM, Johnson NR, Levy BA, Stuart MJ, Krych AJ. Lateral meniscus allograft transplantation: the bone plug technique. *Arthrosc Tech.* 2017;6(4):e1215-20. doi: 10.1016/j.eats.2017.04.016.
28. Ambra LF, Mestriner AB, Ackermann J, Phan AT, Farr J, Gomoll AH. Bone-Plug Versus Soft Tissue Fixation of Medial Meniscal Allograft Transplants: A Biomechanical Study. *Am J Sports Med.* 2019;47(12):2960-5. doi: 10.1177/0363546519870179.
29. Ahmed AM, Burke DL. In-vitro measurement of static pressure distribution in synovial joints--Part I: Tibial surface of the knee. *J Biomech Eng.* 1983;105(3):216-25. doi: 10.1115/1.3138410.
30. Kim JG, Lee YS, Bae TS, et al. Tibiofemoral contact mechanics following posterior root of medial meniscus tear, repair, meniscectomy, and allograft transplantation. *Knee Surg Sports Traumatol Arthrosc.* 2013;21(9):2121-5. doi: 10.1007/s00167-012-2182-4.
31. Lee SJ, Aadalen KJ, Malaviya P, et al. Tibiofemoral contact mechanics after serial medial meniscectomies in the human cadaveric knee. *Am J Sports Med.* 2006;34(8):1334-44. doi: 10.1177/0363546506286786.
32. McDermott ID, Lie DTT, Edwards A, Bull AMJ, Amis AA. The effects of lateral meniscal allograft transplantation techniques on tibio-femoral contact pressures. *Knee Surg Sports Traumatol Arthrosc.* 2008;16(6):553-60. doi: 10.1007/s00167-008-0503-4.
33. Zaffagnini S, Di Paolo S, Stefanelli F, Del Fabbro G, Macchiarella L, Andrea Lucidi G, et al. The biomechanical role of meniscal allograft transplantation and preliminary in-vivo kinematic evaluation. *J Exp Orthop.* 2019;6(1):27. doi: 10.1186/s40634-019-0196-2.
34. Pellegrino M, Trinchese E, Bisaccia M, et al. Long-term outcome of grade III and IV chondral injuries of the knee treated with Steadman microfracture technique. *Clin Cases Miner Bone Metab.* 2016;13(3):237-40. doi: 10.11138/ccmbm/2016.13.3.237.
35. Haut Donahue TL, Hull ML, Rashid MM, Jacobs CR. How the stiffness of meniscal attachments and meniscal material properties affect tibio-femoral contact pressure computed using a validated finite element model of the human knee joint. *J Biomech.* 2003;36(1):19-34. doi: 10.1016/s0021-9290(02)00305-6.
36. Alhalki MM, Howell SM, Hull ML. How three methods for fixing a medial meniscal autograft affect tibial contact mechanics. *Am J Sports Med.* 1999;27(3):320-8. doi: 10.1177/03635465990270030901.
37. Devaraj AK, Acharya KKV, Adhikari R. Comparison of Biomechanical Parameters between Medial and Lateral Compartments of Human Knee Joints. *Open Biomed Eng J.* 2020;14(1):74-86. doi: 10.2174/1874120702014010074.
38. Wang H, Gee AO, Hutchinson ID, et al. Bone Plug Versus Suture-Only Fixation of Meniscal Grafts: Effect on Joint Contact Mechanics During Simulated Gait. *Am J Sports Med.* 2014;42(7):1682-9. doi: 10.1177/0363546514530867.
39. Vrancken AC, Eggermont F, van Tienen TG, et al. Functional biomechanical performance of a novel anatomically shaped polycarbonate urethane total meniscus replacement. *Knee Surg Sports Traumatol Arthrosc.* 2016;24(5):1485-94. doi: 10.1007/s00167-015-3632-6.

40. Paletta GA, Manning T, Snell E, Parker R, Bergfeld J. The effect of allograft meniscal replacement on intraarticular contact area and pressures in the human knee. A biomechanical study. *Am J Sports Med.* 1997;25(5):692-8. doi: 10.1177/036354659702500519.
41. Dienst M, Greis PE, Ellis BJ, Bachus KN, Burks RT. Effect of lateral meniscal allograft sizing on contact mechanics of the lateral tibial plateau: an experimental study in human cadaveric knee joints. *Am J Sports Med.* 2007;35(1):34-42. doi: 10.1177/0363546506291404.
42. Sekaran SV, Hull ML, Howell SM. Nonanatomic location of the posterior horn of a medial meniscal autograft implanted in a cadaveric knee adversely affects the pressure distribution on the tibial plateau. *Am J Sports Med.* 2002;30(1):74-82. doi: 10.1177/03635465020300012601.
43. Maher SA, Wang H, Koff MF, Belkin N, Potter HG, Rodeo SA. Clinical platform for understanding the relationship between joint contact mechanics and articular cartilage changes after meniscal surgery. *J Orthop Res.* 2017;35(3):600-11. doi: 10.1002/jor.23365.
44. Dean CS, Olivetto J, Chahla J, Serra Cruz R, LaPrade RF. Medial meniscal allograft transplantation: the bone plug technique. *Arthrosc Tech.* 2016;5(2):e329-35. doi: 10.1016/j.eats.2016.01.004.
45. Southworth TM, Naveen NB, Tauro TM, Chahla J, Cole BJ. Meniscal Allograft Transplants. *Clin Sports Med.* 2020;39(1):93-123. doi: 10.1016/j.csm.2019.08.013.
46. Yow BG, Donohue M, Tennent DJ. Meniscal Allograft Transplantation. *Sports Med Arthrosc.* 2021;29(3):168-72. doi: 10.1097/JSA.0000000000000302.
47. Abat F, Gelber PE, Erquicia JI, Tey M, Gonzalez-Lucena G, Monlau JC. Prospective comparative study between two different fixation techniques in meniscal allograft transplantation. *Knee Surg Sports Traumatol Arthrosc.* 2013;21(7):1516-22. doi: 10.1007/s00167-012-2032-4.
48. Griffin TM, Guilak F. The role of mechanical loading in the onset and progression of osteoarthritis. *Exerc Sport Sci Rev.* 2005;33(4):195-200. doi: 10.1097/00003677-200510000-00008.
49. Andriacchi TP, Mündermann A, Smith RL, Alexander EJ, Dyrby CO, Koo S. A framework for the in vivo pathomechanics of osteoarthritis at the knee. *Ann Biomed Eng.* 2004;32(3):447-57. doi: 10.1023/b:abme.0000017541.82498.37.
50. Aigner T, Sachse A, Gebhard PM, Roach HI. Osteoarthritis: pathobiology-targets and ways for therapeutic intervention. *Adv Drug Deliv Rev.* 2006;58(2):128-49. doi: 10.1016/j.addr.2006.01.020.
51. A Cavendish P, DiBartola AC, Everhart JS, Kuzma S, Kim WJ, Flanigan DC. Meniscal allograft transplantation: a review of indications, techniques, and outcomes. *Knee Surg Sports Traumatol Arthrosc.* 2020;28(11):3539-50. doi:10.1007/s00167-020-06058-6.